

# Spatio-Temporal Bandwidth-Based Segmented Acquisition for Dynamic 3D Contrast-Enhanced Breast MRI

Sumati Krishnan, Jeffrey A. Fessler, Thomas L. Chenevert

Department of Biomedical Engineering, University of Michigan, Ann Arbor MI 48109

## Introduction

Dynamic contrast enhanced (DCE-MRI) of the breast should ideally be performed at high temporal and high spatial resolution to evaluate both enhancement dynamics and lesion spatial-architectural features (1,2). There is, however, an inherent tradeoff between the maximum achievable temporal and spatial resolution (3). In this work, a formalism is presented that considers the dual bandwidth properties of an object's spatial and temporal enhancement features, in devising a segmented k-space 3D ( $N_x$  readout,  $N_y$   $N_z$  phase encode) acquisition scheme.

## Methods

In this formalism, the slowest phase-encoding axis, say  $k_y$ , is chosen as the axis along which k-space traversal will be traded for increased temporal sampling. Therefore, in the initial analysis a simple 1-D temporally modulated object is considered. Let  $M(y)$  represent the object spatial features which are separable from the temporal features given by  $C(t)$ , simulated to show breast lesion-like enhancement using a pharmacokinetic model (4), (Fig 1.). The sampling bandwidth criteria will be determined by analyzing the " $k_y - k_t$ " Fourier domain of this composite spatio-temporal object (Fig 2.). For a given TR, rate of digitization along  $k_y$  is given by,  $Rk_y = 1/(TR \cdot N_z)$ . If  $T_{max}$  is the overall imaging duration, then maximum number of  $k_y$  samples that can be acquired is,  $N_{max} = T_{max} \cdot Rk_y$ . Correspondingly, maximum allowable bandwidths are:  $k_{y_{max}} = 1/N_{max}$ ;  $k_{t_{max}} = 1/T_{max}$ . The 2-D  $k_y - k_t$  spectral map ( $N_{max} \times N_{max}$ ) is generated, by taking the outer product of the Fourier transforms ( $FT(M(y))' \times FT(C(t))$ ) at maximum bandwidth. The optimization criterion for trading off spatial and temporal bandwidths from this dual spectral map is

$$\text{MAX} \left[ \sum_1^{N_{ky}} \sum_1^{N_{kt}} \hat{M}(k_y) \cdot \hat{C}(k_t) \right], \text{ such that } N_{ky} \times N_{kt} \leq N_{max} \quad [1]$$

where,  $\hat{M}(k_y) \cdot \hat{C}(k_t)$  is the instantaneous spectral power in the enhancement modulated object. This yields an area plot within the " $k_y - k_t$ " domain that contains the greatest spectral power for the given spatio-temporal object, constrained by  $N_{max}$  samples. For any given spatial bandwidth included in this area, the corresponding temporal sampling bandwidth can be determined.

This analysis is extended over a selected range of simulated object size and enhancement conditions. Simulations are based on a 3D SPGR sequence with parameters TR = 10ms, TE = 4.6 ms, flip = 40°, matrix = (256x128x32),  $T_{max} = 3'20''$ ,  $N_{max} = 640$ , object dia: 1-40mm, enhancement rate: rapid ( $k = 0.05$ -s), medium ( $k = 0.003$ -s) and slow ( $k = 0.0013$ -s) (4). Over all of the resulting area plots, a histogram of the maximum and mean  $k_t$  bandwidths for discrete segments of  $k_y$ , is obtained. These are used as guidelines to design the segmented acquisition.

## Results and Discussion

A histogram of the resulting temporal bandwidth requirement for 8-line bins in  $k_y$ , is shown in Figure 3. From these results the recommended acquisition would be to sample the central 16  $k_y$  lines at 11-15 temporal samples, the next 16 at 9-13 temporal samples and so on. The  $k_y - k_t$  analysis suggests that k-space traversal should be tailored such that central segments of  $k_y$  are sampled at a high rate and peripheral segments are sampled at a progressively slower rate. This formalism provides an objective

method to design and rank acquisition strategies that address the spatial and temporal resolution tradeoff in DCE-MRI.

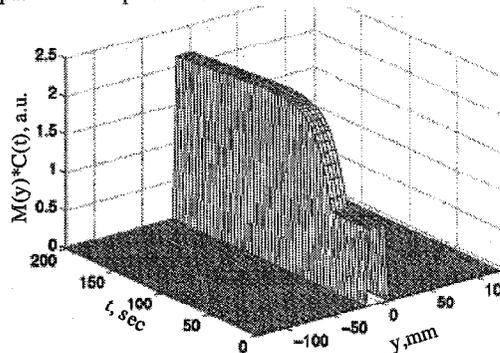


Fig1: Example of combined spatio-temporal object.  $M(y) \cdot C(t)$  is instantaneous contrast modulated spatial object intensity.

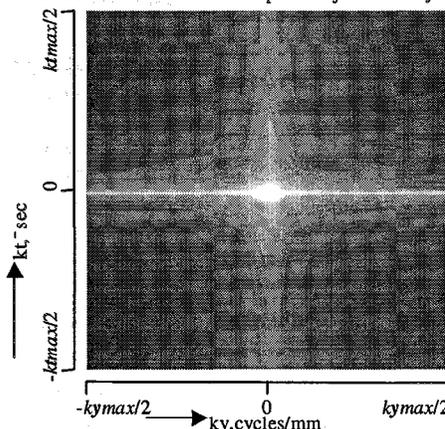


Fig2: Fourier " $k_y - k_t$ " domain representation of spectral power in given spatio-temporal object. Sampling strategy based on maximization of power contained in  $N_{max}$  samples.

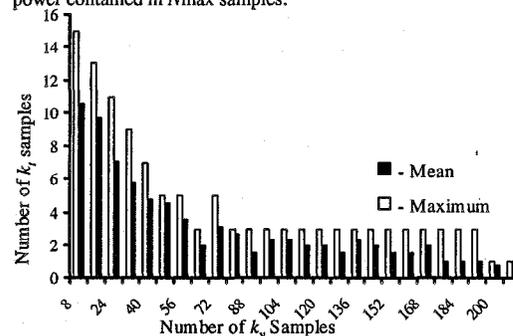


Fig3: Histogram of temporal mean and maximum temporal sampling constraints for discrete segments in  $k_y$  space, over range of spatio-temporal objects.

## References

1. *Clinical Radiology*. 1997;52:516-526
2. *American Journal Roent*. 1997;169:409-415
3. *Radiology*. 196(1):135-42, 1995.
4. *Magnetic Resonance in Medicine*. 33(4):564-8, 1995.